PAUL SCHERRER INSTITUT Center for Proton Therapy :: Paul Scherrer Institut :: #4_11/2014

Dear Colleagues

edition being sent to you one year after the first CNS of young patients treated at PSI with PBSS. of recent studies published by the MDACC/

these very young patients. In the physics' sec- strategies have been assessed and inter-com- quantify the impact of motion on the proton's tion, Ms. Bernatowicz reports quantitative anal-This is an anniversary issue of our SpotOn+, this yses of the effect of motion on (water equivalent) proton range, calculated based on 4D CT data edition in 2013. In the clinical section, the Study for lung and liver tumors. Range maps were and Research Office presents the results of the calculated by converting the CT's Hounsfield Unit atypical teratoid/rhabdoid tumor (ATRT) of the to proton stopping power. Interestingly, the mean range (normalized to end-exhale) de-Although the series is small, it builds to the body creased by 8% and 15% in liver and lung patients respectively. Unfortunately, large variations were Houston and MGH/Boston that suggest that PT observed and the impact of motion was indeed is an effective treatment for young children with case-specific. The second part of the physics As such, re-tracking was simulated and the winter time and a happy new year. Happy holi-ATRT. Of note, 66% of the patient in our series section pertains to a certain type of motion target coverage was improved, nearly achieving days! survived more than 2 years. Importantly, the mitigation strategy, namely tumor tracking in 3 the no motion (i.e. static) dose metrics. These (proxy-rated) quality of life was unaffected in liver cases. More specifically, two beam tracking data are of paramount importance so as to

pared, using 4D dose calculations. The main difference between the two tracking methodologies is that 2D tracking adapts Bragg peaks to the fiducials, while full 3D tracking uses the 3D deformable motion extracted from the model based, motion reconstruction algorithm. Interestingly, dose corruption (i.e. D5-D95) induced by motion could be substantially decreased when 2D or 3D tracking was simulated but could not guarantee an appropriate tumor coverage. I take the opportunity to wish you all a relaxing

range for moving targets and the way to mitigate the effect of motion on target coverage. PSI is committed to perform these analyses and optimize its R&D program, with the aim to treat moving targets in a not too distant future. More information can be found on our website: http://www.psi.ch/protontherapy/center-forproton-therapy-cpt.

Sincerely, Prof. Damien Charles Weber, Head of CPT

Radio-Oncology News

Spot-scanning Proton Therapy for pediatric atypical teratoid/rhabdoid tumors (ATRT): **Clinical outcome of 15 patients treated at PSI**

Dose distribution of a treatment plan superimposed on CT images of a patient with an supra-tentorial ATRT (a axial, b sagital and c coronal views). Note the rapid dose decline between the target and non-target volumes and the optional sparing of contro-lateral brain (coronal and axial slices). The isodose contours are represented by the color-wash (corresponding values are displayed on the right border of each photo).

malignant and extremely aggressive embryonal neoplasm of early childhood. This tumor accounts for 1 – 2% of CNS pediatric tumors but up to 20% of malignant CNS neoplasms in pa-Administered treatments are not ATRT specific and are highly variable but typically includes multi-modality treat- limited but including the recurrence ment, namely surgery, chemotherapy and radiation therapy (RT). Technical improvements in radiation therapy



Atypical teratoid/rhabdoid tumor may improve the therapeutic ratio for (ATRT) of the CNS is a rare, highly these challenging patients. Unlike conventional radiotherapy, proton therapy (PT) allows for optimal dose distributions, with the added benefit of no exit dose. This absence of exit dose has triggered the rational of ustients younger than 3 years of age. ing protons for children with various cancer types.

> We assessed the clinical results, not pattern, toxicity and QoL, of pencil beam scanning (PBS) PT in the treatment of non-metastatic ATRT patients

treated at the Paul Scherrer Institute (PSI). QoL was analyzed by the QoL working group at University of Münster, Germany. The results have been published online (Weber et al 2014). 15 consecutive children with non- metastatic ATRT aged from 4.6 to 27.4 (median, 18.9) months were treated these patients were < 24 months old

months. The localization was infraten- resection (non-gross total resection) resection of the primary tumors was both OS and PFS. achieved in 7 (47%) patients. The Our data suggests that PBS PT is an tients with focal only PT.



torial in 9 (60%) patients. Gross total were negative prognostic factors for

dose administered focally under se- effective treatment for young children dation was 54 Gy (RBE). After a median with ATRT. After PT, with or without Between May 2008 and January 2013, follow-up of 33.4 months (range, 9.7 concomitant chemotherapy, two third -69.2), 3 (20%), 4 (27%) and 2 (13%) of the patients survived > 2 years. patients presented with local failure Importantly, focal only PT, as opposed (LF), distant brain failure (DBF) and to WBI with or without CSI did not rewith PBS PT at PSI. Eighty seven % of spinal failure (SF), respectively. Six sult in an access of distant intracranial patients died, all of tumor progres- failures, the former accounting for treated with focal only chemo-radiaand 20% < 12 months of age. There sion. The 2-year overall- and progres- 20% of all treatment failures. The tion therapy using pencil beam scanwere 7 girls and 8 boys. The majority sion-free survival was 64.6% and acute toxicity was limited and our pro-(n=12; 80%) of tumors were < 5 cm. 66.0%. Tumor location (supratento-spective parental-proxy reporting data ro-Oncology. Published online 02 Nov Mean age at diagnosis was 17.4±7.0 rial; Fig.) and the extent of surgical do not suggest a decrease of QoL of 2014

these very young patients. Late toxicity was unusual. As such, we continue to treat these challenging young pa-

Reference:

Weber et al 2014 Tumor control and QoL outcomes of very young children with atypical teratoid/rhabdoid Tumor ning proton therapy. Journal of Neu-

Medical-Physics News

Characterizing the effect of density variation on proton range in liver and lung as a result of respiratory motion

Background and Methods

Calculated proton ranges depend on density information extracted from the CT images. Density changes appearing due to respiratory deformation are local and temporal variations along the geometrical penetration path need to be quantified for accurate 4D dose calculations. Here, we report a quantitative analysis of the effects of motion on water equivalent range (WER) in proton therapy, calculated based on the 4D-CT images. Additionally, we images (4D-CT(Sim)). 4D-CT(Sim) is interesting for advanced 4D planning, as it generates dose-free images and in the CTV region. Secondly, the corre-

can represent the variability of respira-sponding simulated 4D-CT images were tory motion over multiple breathing created using a static reference CT of cycles.

Firstly, 4D-CTs of three liver and three tracted from the 4D-CT deformable lung patients were evaluated. Changes in tumor and organ volume were calculated and the tumor motion was estimated based on the image data. Single evaluate the effect of using a warped Field, Uniform Dose treatment plans CT image to generate a 4D data set. Similar method is applied to lung pawere calculated using the PSI 3D-TPS. Three single-field plans: P1 – from the tients (data in preparation). right lateral, P2 – posterior oblique, and P3 – posterior were created. Realistic WER maps were then calculated evaluate density effects in simulated by converting the Hounsfield Unit Values to proton stopping power through the whole patient and then evaluated

liver patients and motion data exregistration. Density information from 4D-CT(Sim) and original 4D-CT images was then compared in terms of WER to

Results

As WERs vary over the respiratory cycle, mean WERs were normalized to end-exhale (WER_EE), and were ex-

WER (cm) Field direction



Figure 1 Water equivalent range (WER) calculated for the lung patient at end-inhale (left). The corresponding WER difference (=inhale - exhale) of the same patient. Note largest differences in the CTV occur at the distal edge of the target. Maximum differences (>1cm) were observed around the heart.





tients (covering three different field directions each). In general, mean WER_EE decreased by up to 8 % with inhale in liver patients and about 15 % in lung patients (Fig. 1). Locations exhibiting largest positive/negative differences were identified and analyzed with the WER map. The density infortracted from 4D-CT images of all pa- mation of 4D-CT(Sim) is compared with that of the 4D-CT: an excellent position. This work will be presented agreement was observed, with mean WER differences <3 mm in the liver Treatment Planning Workshop organregion (Fig. 2).

Conclusion

In summary, intrafractional motion affects the beam range in proton therapy. WER variations are case-specific; depend on tumor motion, size and its kinga.bernatowicz@psi.ch



Figure 2 End-inhale liver image from 4D-CT (upper left) and simulated 4D-CT (lower left). The corresponding WER difference (= 4D-CT - 4D-CT(Sim)) of the same patient. Note largest differences occur outside of liver region.

on 28-29th of November at the 4D ized by ICR and UCL in London.

For any further information, please refer to CPT, Kinga Bernatowicz Tel. +41 56 310 5016

Medical-Physics News

Online Image-guided Scanned Beam re-Tracking: necessity and extra benefits

approaches, beam tracking has been considered as the optimal technique, since it should not lead to excessive treatment prolongation or target volume expansions. Due to sequential dose delivery and high sensitivity of proton beams to both small motion and range changes, knowledge on 3D motion in real-time, together with the resultant density variations, is a pre-requisite for clinically implementing such a technique. We have developed an efficient model-based motion reconstruction method (Zhang et al 2013) previously, which allows for online prediction of deformable motion from sparse surrogate motions tracked via an on-board, Beams' Eye View (BEV) X-ray imaging system. Further investigating the feasibility and effectiveness of tumour tracking using pencil beam scanning based on such an image-guided motion compensation approach is the objective of this study (Zhang et al 2014). Two beam tracking strategies have been simulated using 4D dose calculations (4DDC). Conventional 2D tracking laterally adapts Bragg peak positions directly accord-

Among all possible motion mitigation ing to fiducial marker motions tracked from time-resolved BEV images, while 3D tracking utilizes the full, 3D deformable motion extracted from the model based, motion reconstruction algorithm. To reduce the sensitivity of beam tracking to the inevitable uncertainties from both motion tracking and prediction, this study also investigated the potential for 're-tracking' (a combination of re-scanning and tracking), whereby all delivered pencil while also tracking the tumour.

> Due to the relatively large motions This study has demonstrated the feaconsidered, considerable over- and under-dosage can be observed for all cases when no motion compensation is applied. However, the D5-D95 can be substantially reduced to 17, 19 and 29 % or to 15, 18 and 23 % when 2D or 3D beam tracking is employed, compared to the D5-D95 value of 9 % that these gains are mainly evident only for was achieved for the reference (static) plan. Thus, tracking alone (either 2D or 3D) cannot fully recover target dose coverage and homogeneity. By moving but that combining tracking with res- For any further information, to 3x re-scanning (re-tracking), the canning (re-tracking) could provide an robustness has been significantly improved, with even 2D re-tracking pro- aspects of tracking (better dose con- ye.zhang@psi.ch





Figure 2 The relative conformity number in PTV of the 4D plan with different motion mitigation approaches.

of almost comparable quality as the of interplay effects). static plan, together with significant beams are delivered multiple times reductions of the 'inverse interplay effect' in the proximal regions.

> sibility and potential advantages of clinically applying online image-guided scanned beam tracking for mobile tumours treatment. The dosimetric comparison has revealed only a small benefit for deformable 3D beam tracking with respect to 2D tracking, and the larger motions. Our results have also shown that beam tracking alone cannot fully mitigate all motion effects, approach which combines the best Ye Zhang, Tel. +41 56 310 5834

viding dose homogeneities in the PTV formation) and re-scanning (washout

Reference:

- Zhang et al 2013 Deformable motion reconstruction for scanned proton beam therapy using on-line x-ray *imaging*. Physics in Medicine and Biology, Vol. 58(24), pp. 8621-8645
- Zhang et al 2014 Online image guided tumour tracking with scanned proton beams: A comprehensive simulation study. Physics in Medicine and Biology. accepted Oct 2014

please refer to CPT.

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